

Continuous Vagus Nerve Monitoring during Carotid Endarterectomy

Tamaki Tomonori^{1*}, Kubota Minoru², Node Yoji¹, Morita Akio³

¹Departmrnt of Neurological Surgery, Nippon Medical School, Tamanagayama Hospital, Tokyo, Japan ²Department of Clinical Laboratory, Nippon Medical School, Tamanagayama Hospital, Tokyo, Japan ³Departmrnt of Neurological Surgery, Nippon Medical School, Tokyo, Japan

Email: *tamakito@nms.ac.jp

How to cite this paper: Tomonori, T., Minoru, K., Yoji, N. and Akio, M. (2017) Continuous Vagus Nerve Monitoring during Carotid Endarterectomy. Open Journal of Modern Neurosurgery, 7, 1-9. http://dx.doi.org/10.4236/ojmn.2017.71001

Received: August 7, 2016 Accepted: December 9, 2016 Published: December 12, 2016

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Abstract

Backgrounds: Injury to the vagus nerve or one of its branches during carotid endarterectomy can result in vocal fold paralysis but the exact mechanism of injury responsible for vocal fold paralysis after carotid endarterectomy is unclear. Aims: This study was performed to identify potential predictors of vagus nerve injury and obtain feedback by application of intraoperative continuous vagus nerve monitoring. Materials and Methods: Seventy-four patients undergoing carotid endarterectomy were enrolled. A new vagus nerve electrode was designed for less invasive continuous vagus nerve stimulation and monitoring of the vocal fold electromyogram without disturbing the surgical procedure. The device was rectangular (13 mm \times 9 mm), with two small round electrodes set on a flexible silicon plate and tube. The electrode was fully implantable during carotid endarterectomy and was positioned at the most distal site of the vagus nerve by suturing to the connective tissue without nerve dissection. All patients underwent laryngoscopy to assess postoperative vocal fold and pharyngeal wall palsy at one week after carotid endarterectomy. Results: Sudden loss of the vocal fold electromyogram was noted in two patients (during plaque removal and during arterial wall suture in one each). In these two patients, incomplete vocal fold and pharyngeal palsy was confirmed by laryngoscopy. The cause of vagus nerve injury may have been traction at the time of distal internal carotid artery manipulation. The vocal fold electromyogram remained normal during the operation in the other 72 patients. However laryngoscopy revealed postoperative vocal fold and pharyngeal palsy in six patients. These findings suggested that delayed vagus nerve injury can occur after carotid endarterectomy. **Conclusion:** The continuous vagus nerve monitoring may be worthwhile for elucidating the mechanism of vagus nerve injury related to carotid endarterectomy.

Keywords

Carotid Endarterectomy, Vagus Nerve, Vocal Fold, Neuromonitoring, Complication

1. Introduction

Injury to the vagus nerve (VN) is a well-recognized problem in patients undergoing carotid endarterectomy (CEA) [1] [2]. VN damage can lead to undesirable consequences, including vocal disturbance, aspiration, and dysphagia. Although VN palsy is a serious complication of CEA, the causes of VN injury are not well understood [3] [4]. In patients undergoing neck surgery, intraoperative neuromonitoring has been advocated as a method of localizing and identifying the recurrent laryngeal nerve (RLN), as well as being used to predict postoperative vocal fold function [5] [6]. We previously reported a method of intermittent VN monitoring during CEA using a hand-held monopolar electrode for VN stimulation [7]. However, the hand-held stimulator had certain limitations. Besides difficulty in precisely identifying the VN, assessment of functional integrity was limited to the periods of intermittent stimulation. To overcome these limitations, a method that allowed continuous monitoring would be desirable. Accordingly, we performed the present investigation to assess the effectiveness of a new flexible plate electrode for continuous VN monitoring (VNM) by retrospective evaluation in 74 patients undergoing CEA.

2. Materials and Methods

Patients were informed that the continuous VNM system would be employed to assist in localization and identification of the VN, as well as to assess VN function during surgery, and written informed consent was obtained from each patient. There are no financial or professional associations between the authors and the manufacturer of the VNM system. From April 2012 to June 2015, we performed CEA in 96 patients. In 3 patients, continuous VNM could not be done due to technical problems. In addition, we could not identify the VN in 18 patients and 1 patient needed re-exploration for wound hematoma. We excluded these 22 patients. The remaining 74 patients successfully underwent continuous VNM, including 69 men and 5 women aged from 64 to 88 years (mean age: 76 years). Among them, 39 patients underwent right CEA and 35 had left CEA. Induction of anesthesia was achieved with remifentanyl (2 mg/kg) and propofol (2 - 4 mg/kg), and neuromuscular blockade was established. Then a Xomed Nerve Integrity Monitor Electromyogram (EMG) endotracheal tube (Medtronic, Jacksonville, Fila) was inserted by the anesthesiologist. The tube was placed by direct laryngoscopy so that the center of the blue region (indicating the electrodes) was in contact with the true vocal fords and then was it fixed at the angle of the mouth on the non-operated side. Rotation of the tube could be detected by changes of EMG impedance and was corrected by the anesthesiologist. No additional muscle relaxant was given after the first dose. The cuff pressure was maintained at 20 - 22 cm H₂O. After moving the head and neck from the neutral position to full extension, we checked monitor function and the location of the endotracheal tube electrodes by confirming that (1) the impedance was $<25 \text{ k}\Omega$ with an impedance imbalance $<5.0 \text{ k}\Omega$ and (2) there was a normal baseline. The neck was maintained in moderate extension until the end of the operation. In all



patients, CEA was performed by the same standard surgical technique, which involved dissection of the carotid artery while causing the minimum possible damage to any cranial nerves in the operating field. Special attention was paid to careful dissection of the VN from the carotid artery, especially at the sites of proximal and distal clamping. We did not use self-retaining wound retractors. An internal shunt and a Hemashield patch graft were employed in all patients, and the procedure was always performed under an operating microscope. Our intention was to develop a less invasive flexible plate VN stimulation electrode that would not disturb the CEA procedure. The electrode was designed so that dissection of the VN was not required for attachment and so that it remained in contact with the nerve for continuous VNM. Accordingly, two small round stimulation electrodes (cerebral surface electrodes for motor evoked potential monitoring during craniotomy) were placed on a flexible silicon plate and tube (Figure 1). The electrode was fully implantable during CEA and was connected to a Nihon Kohden MEB-2312. Prior to positioning this continuous VNM electrode, we used a conventional handheld bipolar stimulation electrode (stimulus intensity of 0.5 - 2.0 mA, pulse width of 100 µs, and frequency of 3Hz) to identify the VN and we placed the continuous VNM electrode at the most caudal point of the nerve. To maintain contact with the VN, we sutured the silicon plate of the electrode to connective tissue (Figure 2). The stimulus conditions for continuous VNM were as follows: sense: 500 μ V, filter: 2 KHz ~50 Hz, stimulus intensity: <2 mA, single train, duration: 0.2 msec, stimulation rate: 1 Hz, number of stimuli: 10, monitoring time (/div): 20 msec, analysis time (/div): 3 msec, and tend interval: $1 \sim 3$ minutes. The initial stimulus intensity was 0.5 mA using a negative square wave impulse and it was gradually increased in 0.5-mA intervals to the upper limit of 2 mA until the first stable EMG signal from the vocal fold was identified to evaluate the influence of signal amplitude.



Figure 1. This photograph shows the new stimulation electrode for continuous vagus nerve monitoring.



Figure 2. This photograph shows using the new stimulation electrode during carotid endarterectomy.

The Nihon Kohden MEB-2312 was used for both stimulation and measurement, with the latency, amplitude, and duration being assessed as quantitative parameters. Latency was defined as the time (in milliseconds) between the stimulus artifact and the onset of EMG activity and amplitude was defined as the magnitude of the EMG wave (in microvolts). Data are expressed as the mean \pm standard deviation. EMG changes were classified as signal loss (a signal was initially obtained from the VN, but could not be elicited subsequently at 2.5 mA and an event threshold of 100 mV) or impairment (latency delayed by less than 20% and amplitude decreased by less than 50%). For evaluation of cardiac and pulmonary side effects, the heart rate, blood pressure, and SaO₂ were measured before, during, and after continuous VNM. The electrode was removed from the VN just before wound closure. In all patients, vocal fold and pharyngeal movements were observed by laryngoscopy at one week after CEA. When vocal fold dysfunction was identified, follow-up was done at 2-month intervals. We used the Student's t-test for continuous variables and P-values < 0.05 were considered statistically significant.

3. Results

The outcome of surgery was favorable in all patients and none of them developed cerebral ischemia. The mean operating times was 164 min. Heart rate, blood pressure, and SaO₂ did not show significant changes during continuous VNM. Intraoperative electrode dislocation did not occur. The mean continuous VNM time was 68 min (range: 48 - 108 min). A stable initial EMG response could be elicited from 74 VNs during CEA, with a mean supramaximal current of 1.3 mA (range: 0.5 - 2.0 mA). Evoked potentials were successfully recorded from the vocal fold muscle via surface electrodes. Mean values for the left VN obtained by continuous VNM were an amplitude of 474 \pm 142 μ V, latency of 10.3 ± 1.8 ms, and duration of 8.7 ± 2.3 ms, while the mean values for the right VN were an amplitude of 486 \pm 323 μ V, latency of 7.5 \pm 0.8 ms, and duration of 8.4 ± 2.7 ms. The mean latency of the right VN was significantly shorter (p < 0.001) than that of the left VN, whereas the duration and amplitude were similar for both VNs. EMG signal loss occurred in two patients, being noted during plaque removal and during suture of the distal internal carotid artery (ICA) in



one case each (**Figure 3**). In these two patients, we could not detect the EMG by stimulating the VN at any site after signal loss. Laryngoscopy demonstrated incomplete vocal fold and pharyngeal wall palsy, with recovery after 6 months in one patient and 12 months in the other. In the remaining 72 CEA procedures, there was no signal loss or impairment of the vocal fold EMG during continuous VNM. Although six patients showed incomplete vocal fold and pharyngeal palsy on laryngoscopy, they recovered after 2 to 12 months (**Figure 4**). There were no complications of continuous VNM.



Figure 3. The sensory evoked potential (left side) and ipsilateral vocal fold electromyogram (right side) were revealed. The black arrow shows vocal fold electromyogram disappeared suddenly during plaque removing. SEP: Sensory evoked potential, EMG: Vocal fold electromyogram.



Figure 4. This figure shows the sumary of vocal fold electromyogram and laryngoscope findings.

4. Discussion

The reported causes of VN injury during CEA include transection, clamping, stretching, electro-thermal injury, ligature entrapment, and ischemia, but the actual cause of VN injury is often unclear and unproven [1] [2] [8] [9]. Our continuous VNM method is one approach for providing data on the mechanism of VN injury during CEA. In our series, sudden loss of the EMG occurred in two patients during plaque removal and arterial suture, respectively, but not during connective tissue dissection before confirming the VN. The site of VN injury after CEA is important. We previously reported that CEA was associated with injury to the VN trunk in the parapharyngeal space based on data obtained by magnifying laryngoscopy [9]. In the present study, VN injury also affected the nerve trunk in the parapharyngeal space since laryngoscopy revealed vocal fold and pharyngeal wall palsy. A possible mechanism of VN injury during CEA is as follows. The VN trunk in the parapharyngeal space is located near the upper border of the operative field for CEA, just posterior to the internal carotid artery (ICA) [8]. Therefore, ICA manipulation (plaque removal and distal arterial suture in our patients) could stretch the VN together with the vessel and cause traction injury. Six of our patients developed postoperative VN palsy, although the vocal fold EMG was normal at the completion of CEA and impairment of the EMG signal (increasing latency and decreasing amplitude) did not occur intraoperatively. This suggests that VN injury does not only occur during surgery, and that delayed nerve injury is possible after CEA. Such delayed injury to the VN after wound closure could be related to compression by local hematoma or connective tissue edema, or to VN trunk ischemia, and may occur from a few hours to several days after CEA. We previously reported the detection of three cases of Vernet's syndrome by magnifying laryngoscopy after CEA. The glossopharyngeal nerve and accessory nerve are not confirmed during CEA and may sometimes be injured [8]. It is possible that manipulation of the distal portion of the ICA may indirectly damage any of these three nerves (VN, glossopharyngeal nerve, and accessory nerve) by causing edema, swelling, and hemorrhage in the parapharyngeal space. Before this study, we hypothesized that intraoperative impairment of the EMG could provide effective feedback on the effects of surgical maneuvers and predict VN function after CEA, but we did not find such immediate EMG changes and the present monitoring method was not so useful for protecting the VN. There were several limitations of our continuous VNM method. The first limitation was that we could not place the electrode distal to the predicted site of injury to the VN because we usually could not see the nerve in the parapharyngeal space during CEA. Therefore, we could not monitor VN function distal to the predicted site of injury. Second, we could not place the electrode before identifying the VN. Although there were no cases of EMG impairment or failure to obtain a signal at the start of continuous VNM in this series, if the VN was injured before confirmation we would not be able to document the injury. Third, we could not identify the VN in all of our patients and those in whom we were unable to confirm the nerve were excluded from this



study. The overall VN identification rate was 81%. Giovagnorio investigated variations of the VN using ultrasonography [10]. They reported that the VN ran anterior to the common carotid artery in 4.3% of 144 subjects and medial to it in 1.2%. Ha also investigated the variations of VN anatomy, reporting that the nerve ran posterior to the common carotid artery in 13.8% and medial to the vessel in 0.3% [11]. During CEA, the surgeon cannot find a variant VN located medial or posterior to the carotid artery. Visual identification of the recurrent laryngeal nerve (RLN) during thyroid surgery is associated with lower rates of permanent RLN palsy and is considered the gold standard by many authors [12] [13] [14]. Jatzko et al. reviewed 10 reports covering 12,211 thyroid operations and found a lower rate of RLN palsy in the patients with nerve identification than in those without nerve identification (2.7% vs 7.9% for temporary palsy and 1.2% vs 5.2% for permanent palsy) [14]. Especially in patients with visual integrity, the mechanisms of nerve injury are still not well understood [14]. We also must consider the possible side effects of continuous VNM. The same mechanism of VN stimulation was used during continuous VNM as that employed to treat drug-resistant epilepsy and depression [15] [16] [17]. Chronic VN stimulation over several months may lead to side effects, with various types of laryngopharyngeal dysfunction, including hoarseness, cough, pharyngitis, throat discomfort, larvngeal muscle spasm, and dyspnea, being detected after long-term stimulation for weeks or months [15] [16] [17]. However, no complications were seen in our patients after short-term stimulation. In this study, the mean continuous VNM time was 68 minutes, which is a very short duration of VN stimulation, but we cannot exclude the possibility that VN palsy may be induced by continuous VNM. Regarding complete EMG signal loss, the effect of VN fatigue must be considered [18] [19]. However, the lower frequency limit for fatigue of vegetative nerves is more than 10 Hz, while we used 3 Hz for stimulation. In conclusion, continuous VNM was safe and it seems worthwhile to continue investigations in order to elucidate the mechanism of VN injury during CEA.

5. Conclusion

This is the first report of continuous VNM during CEA using new small plated form stimulation electrode. We performed postoperative laryngoscope examination for all cases. From continuous VNM and post CEA laryngoscope findings, we speculated the cause of VN injury was stretch effect during the caudal side ICA manipulation. Although vocal fold EMG was normal at the end point of CEA, there were six cases revealed postoperative VN palsy. These findings created a hypothesis the delayed VN injury mechanism after CEA may exist. The VN monitoring may worth trying for elucidate the mechanism of VN injury of CEA.

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