

3-D EIT Image Reconstruction Using a Block-Based Compressed Sensing Approach

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Received 16 September 2014

Abstract

Electrical impedance tomography (EIT) is a fast and cost-effective technique that provides a tomographic conductivity image of a subject from boundary current-voltage data. This paper proposes a time and memory efficient method for solving a large scale 3D EIT image reconstruction problem and the ill-posed linear inverse problem. First, we use block-based sampling for a large number of measured data from many electrodes. This method will reduce the size of Jacobian matrix and can improve accuracy of reconstruction by using more electrodes. And then, a sparse matrix reduction technique is proposed using thresholding to set very small values of the Jacobian matrix to zero. By adjusting the Jacobian matrix into a sparse format, the element with zeros would be eliminated, which results in a saving of memory requirement. Finally, we built up the relationship between compressed sensing and EIT definitely and induce the CS: two-step Iterative Shrinkage/Thresholding and block-based method into EIT image reconstruction algorithm. The results show that block-based compressed sensing enables the large scale 3D EIT problem to be efficient. For a 72-electrodes EIT system, our proposed method could save at least 61% of memory and reduce time by 72% than compressed sensing method only. The improvements will be obvious by using more electrodes. And this method is not only better at anti-noise, but also faster and better resolution.

Keywords

EIT, Compressed Sensing, Image Reconstruction

1. Introduction

Electrical Impedance Tomography (EIT) [1] is an imaging technique which calculates the electrical conductivity distribution within medium using electrical measurements from a series of electrodes on the medium surface. In this paper, three-dimensional EIT is taken into consideration. Increasing the number of electrodes will increase the number of independent measurements. This increase will provide more impedance information to the measurements. For 3D EIT [2], information required extends to multiple layers; a large number of electrodes could mean better coverage of 3D space. If the number of electrodes increases to 256 electrodes (e.g. 16 planes of 16

electrodes), the number of independent measurement is as high as 64,768. When the problem of a large number of electrodes and a large number of voxels happens, limitations appearing as large size matrices need to be stored and large matrix inversion is required.

This paper proposes a time and memory efficient method for solving a large scale 3D EIT image reconstruction problem and the ill-posed linear inverse problem. We use block-based sampling [3], threshold limits on Jacobian matrix [4] and compressed sensing [5] in 3D EIT reconstruction image. We will introduce this method in the following section.

In this section, we will present shock filter algorithm in detail. Firstly, the X-ray images need to be noise-free images. In order to remove noise of X-ray image, we propose an anisotropic diffusion filter, and it's an adaptive smoothing technique. Secondly, shock filter algorithm is proposed for the X-ray image segmentation and enhancement. Finally, a two-stage shock filter is proposed to optimize the result of shock processing.

2. Block-Based Compressed Sensing in 3-D EIT

In this section, we will illustrate the proposed algorithm in detail. **Figure 1** is the flow chart of block-based compressed sensing algorithm with the improved three steps: block-based sampling, sparse Jacobian matrix and reconstruction algorithm using compressed sensing.

2.1. EIT Image Reconstruction

Most EIT reconstruction methods consider a linear model of the form:

$$y_{M \times 1} = J_{M \times N} \cdot X_{N \times 1} + n \quad (1)$$

where $J \in \mathbb{R}^{M \times N}$ is the Jacobian or sensitivity matrix and $n \in \mathbb{R}^N$ is the measurement noise, which is assumed to be uncorrelated white Gaussian. J is calculated from the FEM as $[y]_{ij} = \frac{\partial [y]_i}{\partial [x]_j}$, and depends on the FEM, the

current injection patterns, the reference conductivity and the electrode models. This system is underdetermined since $\mathbb{R}^N > \mathbb{R}^M$. In order to obtain approximation solution; we need to solve the following minimization problem, which is classical regularization method, called Tikhonov regularization:

$$\arg \min \frac{1}{2} \|y - Jx\|^2 + \lambda \phi(x) \quad (2)$$

where $\lambda > 0$ is the regularization parameter and $\phi(x)$ denotes penalty function or regularization function.

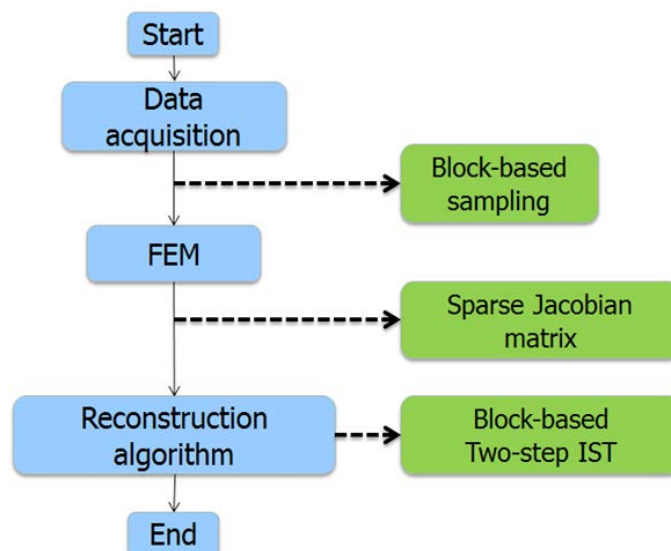


Figure 1. Flow chart of bloc-based compressed sensing algorithm.

2.2. Block-Based Sampling

EIT image is the image of impedance changes. If the measurement data from the specific electrodes has a large of changes, it represents impedance will have a large of changes near the specific electrodes, vice versa. So we want to sample the measurement data of huge changes by using block-based sampling. This method will reduce the size of Jacobian matrix and can improve accuracy of reconstruction by using more electrodes. And then, in order to retain image quality, the paper use the size of 1/3 original signal as our measurement data, e.g. **Figure 2**.

Consider a class S of signal vectors $x \in \mathbb{R}^{JN}$, with J and N integers. This signal can be reshaped into a $J \times N$ matrix, X and we use both notations interchangeably in the sequel. We will restrict entire columns of to be part of the support of the signal as a group. That is, signals in a block-sparse model have entire columns as zeros or non zeros. The measure of sparsity for X is its number of nonzero columns. More formally, we make the following definition (3).

$$S_K = \{X = [x_1 \dots x_N] \in \mathbb{R}^{J \times N} \text{ such that} \\ x_n = 0 \text{ for } n \notin \Omega, \Omega \subseteq \{1, \dots, N\}, |\Omega| = K\} \quad (3)$$

We can extend this formulation to ensembles of J , length- N signals with common support. Denote this signal ensemble by $\{\hat{x}_1, \dots, \hat{x}_J\}$, with $\hat{x}_j \in \mathbb{R}^N, 1 \leq j \leq J$. The matrix \hat{X} features the same structure as the matrix X obtained from a block-sparse signal; thus, the matrix \hat{X} can be converted into a block-sparse vector \hat{x} that represents the signal ensemble. And then, we use the algorithm $\mathbb{S}(X, K)$ to obtain the best block-based approximation of the signal X as follows:

$$X_K^S = \arg \min_{\hat{X}} \|X - \hat{X}\|_{2,2} \text{ s.t. } \|\hat{X}\|_{2,0} \leq K \quad (4)$$

It is easy to show that to obtain the approximation, it suffices to perform column-wise hard thresholding: let ρ be the K th largest L_2 -norm among the columns of. Then our approximation algorithm is

$$\mathbb{S}(X, K) = X_K^S = [x_{k,1}^S \dots x_{k,N}^S]$$

where

$$\mathbb{S}(X, K) = X_K^S = [x_{k,1}^S \dots x_{k,N}^S] \text{ where } x_{k,n}^S = \begin{cases} x_n, & x_n \geq \rho \\ 0, & x_n < \rho \end{cases} \quad (5)$$

for each $1 \leq n \leq N$. Alternatively, a recursive approximation algorithm can be obtained by sorting the columns of X by their L_2 norms, and then selecting the columns with largest norms.

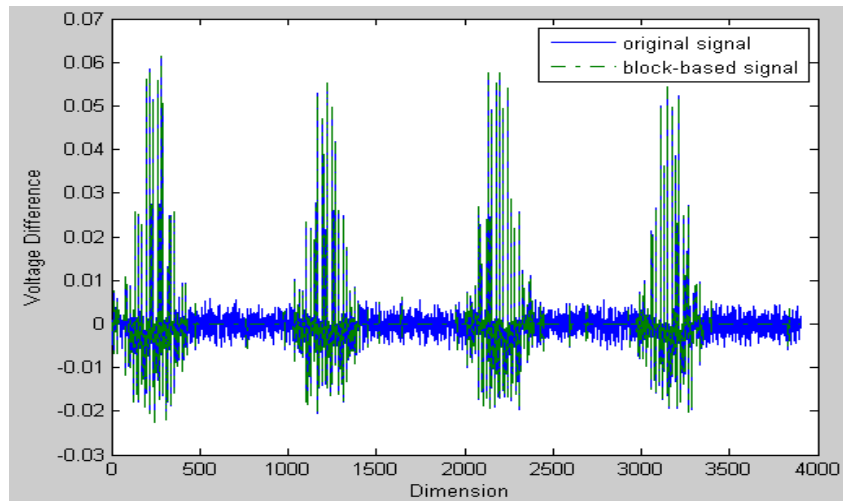


Figure 2. The measurement data is made up of 3904, and a block-based measurement data is made up of 1302 for a 64-electrode EIT system.

Accordingly, the measurement data is reduced so that it is made up of only M_b entries rather than the previous M entries. The Jacobian J_{ij} is now determined for each separate sampled measurement $i = (d, m_b)$ by integrating over finite element Ω_j from the electrical potential calculated in terms of the measured voltage at electrode multiplied by the potential induced by injected current I_d , i.e.,

$$J_b = J_{d,m_b:j} = \frac{\partial V_{d,m_b}}{\partial x_j} = \int_{\Omega_j} \nabla \phi_d \nabla \phi_{m_b} d\Omega \quad (6)$$

where V_{d,m_b} represents the sampled measurements resulting from injected current I_d . Computing the Jacobian by Equation (6) yields a reduced matrix of size $M_b \times N$.

2.3. Sparse Jacobian and Threshold Limits

Due to the nature of 3D EIT, the sensitivity of the measurements to conductivity changes far from the relevant electrodes is small. Those values from the sensitivity map would appear to be very small. The zero elements still remain in the matrix which takes up memory and means they are used in the inverse calculation. The sparse matrix reduction method indicates that values which are very small, typically below a certain threshold, can be belated and transformed to zeros. These zero elements are then eliminated from the Jacobian matrix. This effect would decrease the total number of non-zero elements of the Jacobian matrix hence reducing the memory storage. **Figure 3** shows an example of the effect after thresholding. The level of sparsity (LOS) is defined as the number of non-zero elements divided by the total number of elements in the matrix.

The new Jacobian J_s after being sparsed is then formed:

$$J_s = \begin{cases} J_{ij} & \text{if } J_{ij} \geq t\% \times \overline{\sum J_{\max(h)}} \\ 0 & \text{if } J_{ij} < t\% \times \overline{\sum J_{\max(h)}} \end{cases} \quad (7)$$

where the threshold is $t\%$ of the average value of a sum of h biggest numbers in each row of the Jacobian matrix $\overline{\sum J_{\max(h)}}$. The Jacobian matrix J_s now contains a large amount of zero values.

In order to retain the original image quality, this paper sets the threshold value of 0.5%. And, it can be seen that LOS is at 50% and approximately 50% of total matrix are transformed to zero and can be eliminated.

2.4. Compressed Sensing: Two-Step Iterative Shrinkage/Thresholding Algorithm (TwIST)

This paper uses Two-step iterative shrinkage/thresholding algorithm [6] which are used in compressed sensing [7]. TwIST has been proposed to handle a class of convex unconstrained optimization problems for applications where the observation operator is ill-posed or ill-conditioned. Fortunately, TwIST can actually solve the L_0 regularized LSP which can be expressed as:

$$\arg \min \frac{1}{2} \|y - Jx\|^2 + \lambda \|x\|_0 \quad (8)$$

where λ is the regularization parameter and $\|x\|_0$ is the L_0 -norm of the conductivity changes.

The TwIST algorithm has the form

$$x_1 = \Gamma_\lambda(x_0) \quad (9)$$

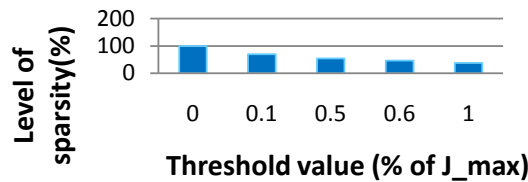


Figure 3. Histogram of the level of sparsity of Jacobian for a 64-electrode EIT system.

$$x_{t+1} = (1-\alpha)x_{t-1} + (\alpha-\beta)x_t + \Gamma_\lambda(x_t) \quad (10)$$

for $t \geq 1$, where $\Gamma_\lambda : \mathbb{R}^m \rightarrow \mathbb{R}^m$ is defined as

$$\Gamma_\lambda(x) = \psi_\lambda(x + J^T(y - Jx)) \quad (11)$$

where ψ_λ is the denoising operator. This paper uses hard threshold function as denoising function. To converge this algorithm, it has the optimal choice of α, β

$$\alpha = \left(\frac{1 - \sqrt{\xi}}{1 + \sqrt{\xi}} \right)^2 + 1 \quad (12)$$

$$\beta = \frac{2\alpha}{1 + \xi} \quad (13)$$

where ξ is the real numbers such that $0 < \xi \leq \lambda_{\min}(J^T J) \leq \lambda_{\max}(J^T J) = 1$. $\lambda_i(\cdot)$ is the i^{th} eigenvalue of its argument.

3. Simulation Results

This paper simulates 3D EIT models by using EIDORS software [8] and modifies EIDORS to use the proposed algorithm introduced in Section 2. All simulation results are performed on a EIT configuration using adjacent current stimulation and voltage measurements. We set sparse jacobian threshold value of 0.5%. 10 dB SNR white Gaussian noise is added in the measurement data.

Figure 4(a) is a 3D EIT model with one circle target. The target is located at $(x, y, z) = (0, 0.1, 0.75)$ and its radius is 0.2. **Figure 4(b)** is a 3D EIT model with two circle target. Two targets are located at $(x, y, z) = (0.5, 0, 0.75)$ and $(-0.5, 0, 0.75)$. Their radiuses are 0.2.

3.1. Analysis of Memory and Time

Figure 5 shows comparison of memory storage and reconstruction time for 4 different methods. We use a 3D EIT model with one circle target at the different number of electrode, and reconstruct them by using 4 different methods. One-step Gauss Newton and Total variation [9] is conventional EIT reconstruction methods. They need use more memory usage and calculation time than compressed sensing algorithm. Less than 56-electrode EIT system, one-step GN is fastest, because there is only the iteration of calculation every computing. For many electrodes, compressed sensing algorithm will meet significant problems regarding storage space and reconstruction time. If we use our proposed improved method in large scale 3D EIT, the problems can be solved effectively. We can use memory efficiently and reduce a lot of reconstruction time.

3.2. Comparisons

The results reconstruct 3D EIT model with one circle target for 48-electrodes and 64-electrodes EIT system, as shown in **Figure 4(a)**. We compare our proposed method with TwIST and use a set of figure of merit to characterize the image qualities based on GREIT [10]. **Table 1** and **Table 2** show that the average value of AR, POS and SD is the same at $z = 0.55 - 0.95$. From the results, 3-D EIT image can retain image quality after using block-based sampling.

Table 3 and **Table 4** show comparison block-based TwIST with one step GN. Block-based TwIST is more robust to noise and the edges of the objects are more clearly defined. These table also show better spatial resolution with our propose method. And then, with conventional method the hyper parameter needs to be optimized with respect to noise level while our method doesn't need such optimization.

Table 1. Comparison of block-based TwIST with original TwIST for 48-electrodes EIT system.

48-electrodes	AR	POS (x, y)	SD
TwIST	467.5308	0.1113, 0.0026	0.1048
Block-based TwIST	467.5308	0.1113, 0.0026	0.1048

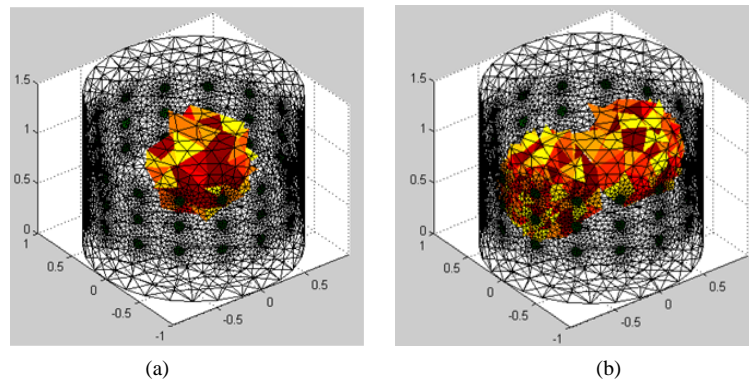


Figure 4. Simulate a 3D EIT model with one and two circle target. (a) One circle target; (b) Two circle target.

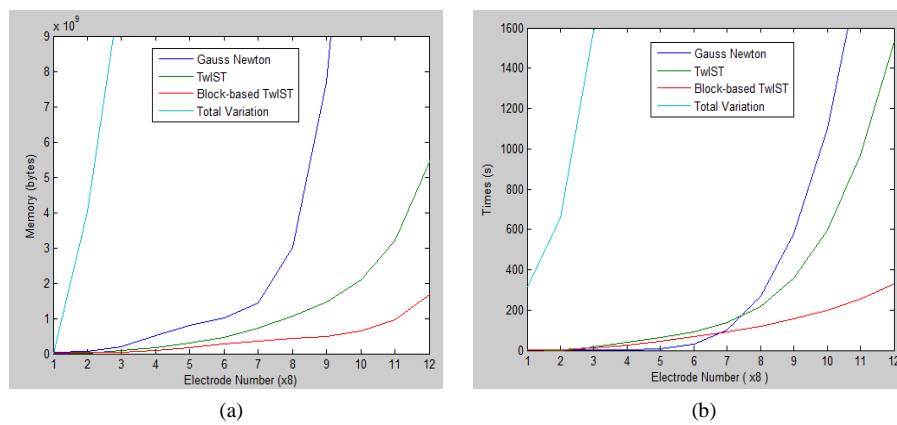


Figure 5. Analysis of memory and time by using 4 different reconstruction image algorithms in 3D EIT. (a) Memory; (b) Time.

Table 2. Comparison of block-based TwIST with original TwIST for 64-electrodes EIT system.

64-electrodes	AR	POS (x, y)	SD
TwIST	379.5438	0.1086, 0.0016	0.4431
Block-based TwIST	379.5438	0.1086, 0.0016	0.4431

Table 3. Different reconstruction results with one circus.

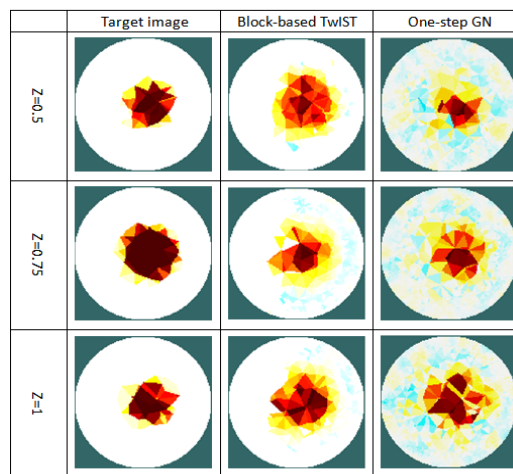
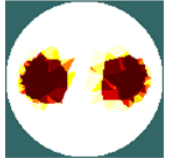
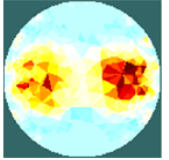
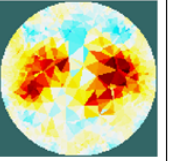
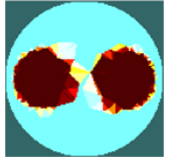
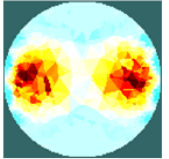
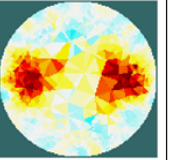
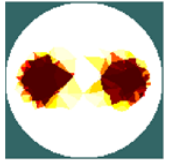
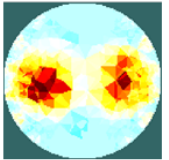
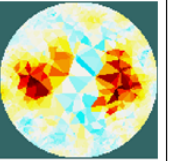


Table 4. Different reconstruction results with two circuses.

	Target image	Block-based TwIST	One-step GN
Z=0			
Z=0.75			
Z=1			

4. Conclusion

In this paper, we presented a time and memory efficient method for solving a large scale 3D EIT image reconstruction problem and the ill-posed linear inverse problem. For a 72-electrode EIT system, our proposed method could save at least 61% of memory and reduce time by 72% than compressed sensing method only. The improvements will be obvious by using more electrodes. And this method is not only better at anti-noise, but also faster and better resolution than the conventional method.

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