# A Rapid Low Power Ultra-Violet Light-Assisted Bacterial Sensor for Coliform Determination

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# ABSTRACT

Titanium dioxide (TiO<sub>2</sub>) particle-incorporated Prussian blue (PB) sensor for the detection and inactivation of *Escherichia coli* (*E. coli*) is developed in this study. The system requires low power ultra-violet (UV) light to photoactivate TiO<sub>2</sub> particles and change of signal response is measured immediately upon irradiation using cyclic voltammetry. The generation of free radical species (OH·) and H<sub>2</sub>O<sub>2</sub> from the oxidation of water by the hole ( $h^+$ ) are the main components which cause destruction of cell membrane and eventually result in the inactivation of cell. Our study also shows direct oxidation of cells by  $h^+$  as one of the mechanisms for cell inactivation due to the close contact between TiO<sub>2</sub> particles and *E. coli* cells. Highly attractive features of this unique sensor include its ability to be regenerated and reused for at least three times without the use of harsh chemicals, good reproducibility and its specificity in bacteria sensing when tested against organic contaminants, which potentially reduce the operation cost when incorporated into water disinfection system. Its superior performance in detection of total coliform without additional steps of sample treatment is also demonstrated in river water. TiO<sub>2</sub> particle-incorporated PB membrane sensor exhibits signal response with higher current output compared to PB-TiO<sub>2</sub> coated screen printed carbon electrode (SPCE) due to its porous structure and higher surface area, suggesting its potential development into a powerful and low cost contamination monitoring tool.

Keywords: Bacterial Sensor; Low Power; Cell Inactivation; E. coli; Coliform; Photocatalysis

# 1. Introduction

Water contamination is one of the most problematic issues where millions of people die from water borne diseases due to the consumption of unsafe or contaminated water. Escherichia coli (E. coli) has been identified as one of the agents for waterborne diseases and its presence in water represents water quality deterioration and contamination by human or animal wastes [1]. This poses serious health risks, such as diarrhea, nausea and other symptoms to consumers, especially infants and those with severely compromised immune system. The contamination of water source by bacteria and pathogen also leads to limited sustainable water supply where one-fifth of world's population has no clean access to water and this scenario is more prominent in developing countries [2]. Hence, there is an urgent need to develop rapid, low cost and simple bacterial sensor with early warning capability and of low power [3,4] in order to address these problems. Electrochemical sensing which is portable and

inexpensive has shown its superior performances in the detection of cells, viruses and biological samples [5-8]. However, real-time detection and regeneration of sensing materials have always been the limitations for biosensing [9]. An electrochemical sensor which exhibits immediate response upon detection and the ability to be reused is expected to be highly useful due to the potential enhanced performance for on-site analysis.

TiO<sub>2</sub> photocatalyst has been used extensively for the photocatalytic degradation of organic compounds for water purification [10,11]. However, the development of photocatalytic reactors remains a challenge due to the high recombination rates of holes and electrons [12] and the lack of ability to regenerate and reuse the material. On the contrary, a polymer incorporated with TiO<sub>2</sub> would be expected to partly resolve the problem of recombination because the polymer serves as the electron acceptor in the conduction band. To develop a low power bacterial sensor, we choose iron hexacyanoferrate polymer which is also known as Prussian blue (PB), incorporated with titanium dioxide (TiO<sub>2</sub>) particles as the sensing material.

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Two electrode configurations, namely porous alumina membrane and screen printed carbon electrode (SPCE) have been employed in this study to investigate the performance of sensor. The polymer incorporated  $TiO_2$  is deposited onto the platinum-coated porous alumina membrane template and SPCE, which act as the working electrode in this study. The setup of polymer-coated membrane sensor operates like a conventional two-electrode electrochemical system but requires only a very low power ultra-violet (UV) lamp to function while SPCE functions as a conventional three-electrode system.

Ultrathin PB film is employed in this work because it can significantly improve the signal response and improve the sensitivity owing to the fast mass transfer of analytes [13,14]. In this study, the sensing of bacteria is carried out without the labeling of antibody as well as with small volume which significantly simplifies the procedures for operation. To further enhance the sensing performance of sensor, large TiO<sub>2</sub> particle size is chosen owing to its good mechanical adhesion [15] and to maximize interaction between particles and bacteria. The two-electrode system used in this work is simple and potentially useful in the application of field measurement conditions. Herein, we utilize a TiO<sub>2</sub> particles incorporated PB film to construct a novel membrane sensor with bacterial sensing capability in small volume of analytes with the aid of low power UV light (Scheme 1). E. coli sensing and detection of total coliform in river water are performed by the sensor using cyclic voltammetry. To further evaluate the application of TiO<sub>2</sub> incorporated PB sensor on E. coli detection, the performance of SPCE coated with PB and TiO<sub>2</sub> is also investigated in this study.

# 2. Experimental

## 2.1. Materials and Instruments

Nanoporous alumina membrane (Anodisc<sup>TM</sup>, 13 mm diameter, 0.02 µm pore size) was purchased from Whatman (Maidstone, Kent, UK). SPCE was obtained from



Scheme 1. Fabrication of the membrane-based bacterial sensor by sputtering ~50 nm thick platinum layer on both sides of 60  $\mu$ m thick nanoporous alumina membrane, followed by coating of TiO<sub>2</sub> incorporated PB film galvano-statically onto the Pt electrode.

Dropsens. The working electrode (4 mm diameter) of SPCE was carbon (C) while the counter and reference electrodes were platinum (Pt) and silver (Ag) respectively. Hydrochloric acid (HCl, 37%) was obtained from P. P. Chemical. Potassium chloride (KCl) was purchased from Sinopharm Chemical Reagent Co. Ltd. Potassium hexacyanoferrate (III) (K<sub>3</sub>Fe(CN)<sub>6</sub>) and Nafion perfluorinated ion-exchange resin were obtained from Sigma-Aldrich. Anhydrous iron (III) chloride (FeCl<sub>3</sub>) was purchased from Merck. Titanium (IV) oxide (TiO<sub>2</sub>, -325 mesh powder, anatase, 99.6%) was obtained from Alfa Aesar. Methanol (MeOH, ≥99.9%) was purchased from Tedia Company, Inc., toluene (C<sub>6</sub>H<sub>5</sub>OH, 99.5%) was obtained from RCI Labscan Limited and 1.4-dioxane  $(C_4H_8O_2, \geq 99.9\%)$  was purchased from Merck. E. coli K12 was obtained from ATCC and it was prepared in 0.01 M phosphate buffered saline (PBS, pH 7.4). All chemicals and solvents were used as received. Ultrapure water (Sartorius Ultrapure Water System) was used for all solution preparation, unless otherwise stated.

Sputter coating of Pt onto the nanoporous alumina membrane was performed by JEOL Auto Fine Coater (JFC-1600). Coating of  $TiO_2$  incorporated PB onto the electrodes and electrochemical measurements were carried out by e-corder 401 (eDaQ) and potentiostat (eDaQ EA161) controlled by a PC.

# 2.2. E. coli Culturing

*E. coli* K12 was purchased from ATCC. Luria Broth (LB) containing 10.0 g tryptone, 5.0 g yeast extract and 10.0 g sodium chloride was used to grow the pure culture of *E. coli*. The culture was grown on an orbital shaker at  $37^{\circ}$ C for 18 h and it was subsequently diluted to 10 cfu·mL<sup>-1</sup> with 0.01 M PBS, pH 7.4. *E. coli* cell number was enumerated by spread plate method where 0.1 mL of diluted solution was spread evenly on LB agar plate and incubated at  $37^{\circ}$ C for 24 h. *E. coli* colonies on the plates were counted for determination of the number of viable cell in colony-forming units per milliliter (cfu·mL<sup>-1</sup>).

# 2.3. River Water Spiking

One-liter of water sample was collected from Kallang river, Singapore on 16 Jan 2013. The water sample was divided into three equal volumes and two of the solutions were spiked with different volumes of 30 cfu·mL<sup>-1</sup> *E. coli* solution to make up the desired spiked concentration. All solutions were finally made up to equal volumes using PBS. The electrochemical measurement was then carried out according to the procedures stated below.

#### 2.4. Sensor Fabrication

Fabrication of  $TiO_2$  incorporated PB membrane sensor was based on the procedure described elsewhere [16].

Both sides of the nanoporous alumina membrane were sputtered with conductive Pt layers and it was subsequently electrodeposited with PB (Scheme 1). The active side of the sputtered membrane served as the working electrode while the passive side of the membrane as counter electrode and silver/silver chloride (Ag/AgCl) in 1 M KCl was used as the reference electrode during the coating process. The membrane was coated using galvanostat for 1 h in an aqueous solution of 20 mM K<sub>3</sub>Fe(CN)<sub>6</sub> and 20 mM FeCl<sub>3</sub> with pH adjusted to be around 2.0 using HCl. TiO<sub>2</sub> particles were suspended in the same solution with a concentration of 15  $g \cdot dm^{-3}$ . The solution was stirred and dropped onto the surface of membrane every 10 min to ensure that TiO<sub>2</sub> was coated together with PB. The current density was 20 µA·cm<sup>-2</sup> and total electrolysis charge passed was 72.2 mC·cm<sup>-2</sup>. The TiO<sub>2</sub> incorporated PB membrane was then rinsed with ultrapure water and dried overnight at room temperature. The passive side of the membrane was coated with Nafion before it was used for sensing. The coating of SPCE was accomplished by the same procedures except Pt and Ag were used as the counter and reference electrodes respectively.

### 2.5. Sensing and Disinfection of E. coli

*E. coli* sensing was carried out by spreading 20  $\mu$ L of *E. coli* solution on both sides of the membrane and the working electrode of SPCE prior to irradiation and signal response was obtained from cyclic voltammogram (CV). The sensor was then subjected to UV light irradiation which the source was a 4 W money detector (MD401, Khind) before the determination of electrochemical response. After the first measurement, the sensor was rinsed with copious amount of PBS to remove bacteria from the previous scan. Higher concentration of *E. coli* solution was applied onto the sensor and the signal response was determined again. The electrochemical measurement system comprised an integrated two-electrode setup or SPCE as well as e-corder 401 (eDaQ) and potentiostat (eDaQ EA161) controlled by a PC.

#### 3. Results and Discussion

#### 3.1. Model for Bacterial Sensor Signal Response

The TiO<sub>2</sub> incorporated PB membrane sensor presents a large signal response toward *E. coli* solution upon irradiation in contrast to the signal response before exposure of light (**Figure 1(a)**). This remarkably high electroactivity of bacterial sensor cannot be observed on sensor in the absence of PB films (**Figure 2(a)**) because electron transfer is harder to occur in TiO<sub>2</sub> due to its larger band gap of 3.2 eV [17]. The change of peak current is insignificant when PB sensor without TiO<sub>2</sub> is used (**Figure 2(b**)). This clearly indicates that bacteria sensing happens

only when there are photogenerated electrons and highly reactive radical species from  $TiO_2$  particles. Further evaluation of the sensor in differentiating its signal response from organic compound, methanol reveals insignificant change of signal response (**Figure 1(b)**). The difference in electrochemical behaviors can be explained by the chemical reaction of PB and methanol [18] causing the PB film to dissolve away thereby, reducing electrochemical activity.

The significantly high oxidative current of bacterial sensor upon irradiation is owing to the formation of Prussian white (PW) as a result of injection of photoexcited electron into PB as shown in **Scheme 2**. A hole  $(h^+)$  and electron  $(e^-)$  pair is generated in the valence and conduction bands respectively when TiO<sub>2</sub> is illuminated with light of appropriate wavelength (300 - 400 nm). The valence band  $h^+$  reacts with water molecule to produce hydroxyl radical (OH·) and the recombination of OH· produces hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>). To prevent the ex-



Figure 1. Cyclic voltammogram of TiO<sub>2</sub> incorporated PB membrane sensor with (a) 20  $\mu$ L 10 cfu·mL<sup>-1</sup> of *E. coli* before ( ......) and after ( - · - ) UV light irradiation (b) 20  $\mu$ L of methanol before ( -- · - ) and after ( --- ) UV light irradiation. Conditions: scan rate = 20 mV·s<sup>-1</sup>, potential range = -0.4 to 0.4 V, *E. coli* concentration = 10 cfu·mL<sup>-1</sup>, methanol concentration = 20% (v/v).



Figure 2. Cyclic voltammogram of (a) TiO<sub>2</sub> sensor without PB before ( \_\_\_\_\_\_) and after ( \_\_\_\_\_\_) irradiation; (b) PB sensor without TiO<sub>2</sub> before ( \_\_\_\_\_\_) and after ( \_\_\_\_\_\_) irradiation. Conditions: scan rate = 20 mV·s<sup>-1</sup>, potential range = -0.4 to 0.4 V, *E. coli* concentration = 10 cfu·mL<sup>-1</sup>.

tremely deleterious  $e^- - h^+$  recombination reaction, PB with compatible band gap energy [19] was chosen to TiO<sub>2</sub> particles as the bacteria sensing material. In this study, the bacteria sensing is proposed to be coupled with disinfection of bacteria, where highly reactive OH and H<sub>2</sub>O<sub>2</sub> are responsible for cell wall decomposition, subsequently change the cell membrane permeability [20-24]. Hence, the disinfection of *E. coli* is mainly due to the destruction of cell wall and followed by cell membrane which permeability change allows the penetration of highly reactive species into the cytoplasmic membrane. Direct oxidation of cells by  $h^+$  has also been proposed previously but the detailed mechanism has not been discussed extensively [24,25].

#### 3.2. Analytical Performance of Bacterial Sensor

Figure 3 illustrates the correlation between oxidative current with increasing concentration of E. *coli* upon irradiation. The bacterial sensor shows significant change of response upon irradiation and the short analysis time

outperforms the conventional methods for detection of *E*. *coli* in water, including multiple-tube fermentation and membrane filter techniques which require time-consuming and labor-intensive procedures [26]. The correlation between logarithm concentration of *E. coli* and oxidative peak current is somewhat linear between 10 to  $10^5$  cfu·mL<sup>-1</sup> (**Figure 3**) and it can be established using the equation:

$$\frac{I_{\rm p} - I_{\rm p,0}}{k_1} = \log \frac{[c]}{k_2} \tag{1}$$

where  $I_p$  and  $I_{p,0}$  are the oxidative peak currents in the presence and absence of *E*. *coli*,  $k_1$  and  $k_2$  are constants and [*c*] is the concentration of *E*. *coli*.

The calibration plot is obtained from three independent sets of experiments with three different sensors. The increase contact between TiO<sub>2</sub> particles and higher concentration of *E. coli* explains the relationship of signal response and *E. coli* concentration [24]. The  $h^+$  generated can react with cells [25] more rapidly and it can also be filled more readily by electrons generated from the decomposition of cells which have close contact with TiO<sub>2</sub> particles [24]. Whereas for lower concentration of cells, less cells can be oxidized by the  $h^+$  thus, resulting in lower oxidative current. This suggests direct oxidation of cells as one of the mechanisms occurring in our study of cell disinfection.

#### **3.3. Interference Study**

The effect of organic contaminants on the sensor is evaluated with three organic compounds, toluene, methanol and 1,4-dioxane which are commonly found in industrial effluent and ground water contaminated by point emissions [27-29]. All sensor signal responses are derived from the peak currents of the potential scans and offset against the potential scan obtained in the absence of E. coli cells. Figure 4 reveals the sensor signal response toward E. coli, mixture of E. coli with organic contaminants and 1 h after suspension of E. coli in the organic mixtures. The sensor was first applied with 10  $cfu \cdot mL^{-1}$ E. coli solution to obtain the signal response. A mixture of three organic compounds, 0.05 ppm 1,4-dioxane, 0.002 ppm methanol and 0.002 ppm toluene were then added into the E. coli solution and applied onto the sensor to obtain the second signal response. These concentrations were chosen because these are the possible levels of contaminants present in polluted water [27-29]. There is insignificant change of signal response even after the sensor was exposed to organic contaminants, demonstrating that the presence of organic contaminants does not passivate nor interfere with the sensor performance on bacteria sensing. After 1 h suspension of E. coli in organic mixtures, the solution was applied onto the sen-



Scheme 2. Schematic diagram of principle of operation of bacterial sensor and photocatalytic inactivation of *E. coli* by TiO<sub>2</sub> under UV light irradiation.



sor to acquire the next signal response. The difference in signal observed might be attributed to the mineralization of organic compounds by *E. coli* after prolonged mixing, contributing to slight increase in signal response [30]. This sensor shows its superior performance in *E. coli* detection even in the presence of organic contaminants, which are known to react with TiO<sub>2</sub> [10,11], leading to its potential application in contaminated water analysis.

## 3.4. Reproducibility and Regeneration of Bacterial Sensor

The reproducibility of the fabrication procedure was determined by coating PB incorporated  $TiO_2$  onto platinum sputtered porous alumina membrane under identical conditions and measured the signal response toward 10  $cfu \cdot mL^{-1} E. coli$ . The coefficient of variation of fabrication reproducibility for three different sensors was found to be within 8%.

To investigate the reusability of the bacterial sensor, change of signal response before and after irradiation was monitored at 10 cfu·mL<sup>-1</sup> *E. coli* in three independent experiments. After each analysis, the sensor was immersed in PBS for 10 min to ensure that bacteria cells had detached from the sensor prior to the next experiment. Single factor ANOVA test shows that there is no significant difference of the sensor signal response at 95% confidence level. As shown in **Figure 5**, the sensors can be readily regenerated after rinsing with PBS solution and this presents an outstanding feature of the sensor since reusability has always been regarded as one of the most important features of bacterial biosensors for practical use [31].

#### 3.5. Applications of Bacterial Sensor

To demonstrate useful applications of bacterial sensor for the analysis of total coliform in freshwater samples, analysis was conducted using untreated river water samples collected in clean sterile containers and subsequently spiked with 30 cfu·mL<sup>-1</sup> *E. coli*. The *E. coli* concentration in the water sample was analyzed by comparing the TiO<sub>2</sub> incorporated PB membrane sensor signal response to the standard calibration curve constructed in **Figure 3**. Real sample analysis of total coliform in river water samples shows excellent correlation of spiked concentrations and experimentally determined values at 95% confidence level. The sensor developed therefore can be applied for sensing and deactivation of bacteria in river water and it can also be widely used in the analysis of water samples from other sources.

Performance of the sensor was then evaluated on nonporous electrode, SPCE to compare with that of porous



Figure 4. Change of oxidative peak current of TiO<sub>2</sub> incorporated PB membrane sensor  $(I_p - I_{p,0})$  toward *E. coli*, *E. coli* + organics 1 (*E. coli* in a mixture of methanol, toluene and 1,4-dioxane) and *E. coli* + organics 2 (*E. coli* incubated in a mixture of methanol, toluene and 1,4-dioxane for 1 h).  $I_p$  represents the peak current signal in the presence of *E. coli* and *E. coli* in the mixture of organics upon irradiation while  $I_{p,0}$  represents peak current signal before irradiation. Conditions: scan rate = 20 mV·s<sup>-1</sup>, potential range = -0.4 to 0.4 V, *E. coli* concentration = 10 cfu·mL<sup>-1</sup>, methanol concentration = 0.002 ppm, toluene concentration = 0.002 ppm, 1,4-dioxane concentration = 0.05 ppm.



Figure 5. Change of oxidative peak current of TiO<sub>2</sub> incorporated PB membrane sensor  $(I_p - I_{p,0})$  toward *E. coli* for three different sets of experiments.  $I_p$  represents signal response after *E. coli* was applied onto the sensor followed by irradiation while  $I_{p,0}$  represents the signal response before irradiation. Conditions: scan rate = 20 mV·s<sup>-1</sup>, potential range = -0.4 to 0.4 V, *E. coli* concentration = 10 cfu·mL<sup>-1</sup>.

alumina membrane electrode. **Figure 6** gives the signal response of PB-TiO<sub>2</sub> coated SPCE with increasing concentration of *E. coli*. The correlation between logarithm concentration of *E. coli* and peak current follows Equation (1) and the linear range from 10 to  $10^5 \text{ cfu} \cdot \text{mL}^{-1}$  is established. However, the current range obtained from PB-TiO<sub>2</sub> coated SPCE is lower that than of TiO<sub>2</sub> incorporated PB membrane sensor due to its non-porous structure and smaller surface area [32]. This suggests the highly regular, rigid and dense porous material with high pore density favors high PB loading and it can also act as reservoir of PB that restricts PB leaking, resulting in higher current range [33].



Figure 6. Cyclic voltammogram of PB-TiO<sub>2</sub> coated SPCE before irradiation ( .........) and after irradiation in the presence of 10 cfu·mL<sup>-1</sup> ( – – – ),  $10^2$  cfu·mL<sup>-1</sup> ( – – ),  $10^3$  cfu·mL<sup>-1</sup> ( – – – ),  $10^4$  cfu·mL<sup>-1</sup> ( – – – ),  $10^5$  cfu·mL<sup>-1</sup> ( – – – ),  $1^5$  cfu·mL<sup>-1</sup> ( – – – – ),  $1^5$  cfu·mL<sup>-1</sup> ( – – – ),  $1^5$ 

#### 4. Conclusion

In conclusion, we describe a unique bacterial sensor comprising PB coated porous membrane or SPCE electrode incorporated with TiO<sub>2</sub> particles which demonstrate high sensitivity bacterial sensing utility and simultaneously, deactivate the bacteria. Unlike other detection methods which require lengthy incubation time, this sensor exhibits change of signal response immediately after the application of E. coli solution onto the sensor and at the start of detection procedure. The sensor also shows its specificity towards E. coli when tested against organic contaminants which are commonly present in industrial effluent and polluted groundwater and this feature is extremely useful in the monitoring of water quality which bacteria act as the contamination indicators. The simple integrated two electrode setup of TiO<sub>2</sub> incorporated PB membrane sensor shows its superior analytical performance in detection of total coliform in water sample derived from river water. In addition, the higher current output of membrane sensor at low analyte concentrations as compared to PB-TiO<sub>2</sub> coated SPCE suggests its potential development into low cost and portable water disinfection system which can be highly applicable in developing countries where UV irradiation is readily available. Because of the potential ease of miniaturizing of the two electrode setup, this sensor could be developed into a powerful contamination monitoring tool for on-site analysis of water from various sources.

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